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A Robust MR Image Segmentation Method for Enhanced Brain Tumor Detection

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ABSTRACT

In medical image analysis, the segmentation of brain tumors is a crucial component in treatment, encompassing tasks such as tumor identification, patient follow-up, and computer-guided surgery. To enhance treatment outcomes and increase the survival rates of subjects, it is essential to leverage pertinent information provided by magnetic resonance imaging (MRI). MRI, as an advanced imaging technique, provides comprehensive and pertinent information, including details about the size, location, and shape of brain tumors. However, the detection of brain tumors has been a challenging task due to the complex features in their appearance and boundaries. The focus of this paper is on presenting an image segmentation technique for the detection of brain tumors. The proposed work is delineated into three phases. In the initial phase, we employ an optimization approach to segment brain tissue using Fuzzy Particle Swarm Optimization. The second phase utilizes a fuzzy approach to identify brain tumors through Fuzzy C-Means. The third phase integrates the results from the previous steps and incorporates a qualitative reasoning model based on Mamdani fuzzy logic is integrated with an optimized rule set for precise brain tumor diagnosis. The results obtained indicate that the proposed approach significantly outperforms existing techniques, achieving a sensitivity of 92%, a specificity of 97%, and an accuracy of 99.71%.

1. INTRODUCTION

The brain serves as the central hub of the nervous system. It is composed of spongy and non-replaceable soft tissues [1, 2]. Various diseases, including brain tumors, can impact the brain. The brain tumor is a collection of atypical cells which proliferate rapidly within the brain. Several types of brain tumors exist, classified into two primary groups: noncancerous (benign) brain tumors, which are less aggressive, develop slowly, and typically remain confined to the surrounding normal brain tissues; and malignant brain tumors (cancerous), which pose a challenge in distinguishing them from the adjacent normal tissues [3]. Different malignant tumors (e.g., astrocytoma. glioma, meningioma, metastatic, medulloblastoma tumors) exhibit significant differences in their appearance, size, and location [4]. Detecting brain tumors remains an unresolved challenge due to the intricate nature of their structure [5].

In medical imaging, the MRI method is employed to retrieve comprehensive information about the internal tissues of a specific body part [6]. MRI provides a variety of series, comprising T2-weighted, T1-weighted, and proton density images (PD), offering a comprehensive view of internal

structures [7]. In the investigation of brain tumors, precise localization is vital as it plays a significant role in discovering the shape and tumor size. Hence, numerous segmentation approaches and techniques have been introduced in the literature to achieve accurate tumor extraction.

Image segmentation is a vital and pivotal step in comprehending images, extracting features, and examining and interpreting them for diverse applications. It finds common applications in medical science, including tissue classification, tumor identification, and estimation of tumor volume, surgical planning, and delineation of blood cells, image registration, and atlas matching [8]. For instance, it is instrumental in the pathological identification of brain abnormalities and the uncovering of tumors from MRI images [9]. Brain tumor segmentation involves distinguishing different tumor tissues from typical brain tissues, including gray matter (GM), cerebrospinal fluid (CSF), and white matter (WM) [10, 11]. Image segmentation has a pivotal role in various phases, including treatment planning, surgical navigation, and disease diagnosis, highlighting its significant impact in the medical field. Planning an efficient and robust segmentation algorithm for brain tumor has become an essential step in the process [12]. This essential role of image segmentation has become increasingly prominent, serving as a cornerstone in image processing that significantly enhances the efficiency of clinicians during the medical diagnosis process [13]. Automated brain tumor detection, classification, and segmentation using MRI information primarily rely on a fully automated tumor segmentation method for extracting areas, providing an improved classification of brain tumors, and ultimately aiding in the early and precise discovery of brain tumors [5].

This paper presents a novel approach to enhance and refine the process of brain tumor detection and segmentation, focusing on improving both efficiency and accuracy. The proposed framework removes the necessity of expert intervention and combines the FPSO and FCM algorithms, leveraging the strengths of both methods and mitigating their respective drawbacks. In the final phase, when the FCM algorithm detects lesions as outlier tissues, a decision-making system based on a Mamdani fuzzy inference model is applied.

The paper is structured as follows: Section II provides a review of prior research on tumor segmentation in MRI. Section III describes the methodology proposed in this work. Section IV provides and analyzes the experimental results. Finally, Section V offers the conclusions of the study.

2. RELATED WORK

In recent years, various research approaches have been explored and are still evolving, aiming to propose an effective, robust, and accurate automatic segmentation tool for brain tumors [13]. However, this observation not only underscores the demand for automated tools in brain tumor segmentation but also emphasizes that research in this area is an ongoing work in progress [13]. Segmentation methods for brain tumors, particularly those focused on MRI, can be broadly categorized into three classes: (i) manual methods, (ii) interactive (semi-automatic) approaches, and (iii) fully-automatic techniques [14-16].

Brain tumors manual segmentation demands the expertise and knowledge of multiple clinicians to manually define the tumors. Consequently, this task is deemed tedious and time-consuming. When conducted by experts, manual segmentation is subject to intra and inter-rater inaccuracies. Therefore, fuzzy ranges are established when estimating the segmentation to account for such variability [15]. Manual segmentations are typically used to assess the accuracy of semi-automatic and fully automatic methods [17].

Human participation in semi-automated brain tumor segmentation is frequently needed to initiate the segmentation process, assess the accuracy of the segmentation result, or manually guide the segmentation outcome [13]. Generally, existing research focuses on semi-automatic-based segmentation of brain tumors with the objective of minimizing human interaction to the greatest extent possible [10]. The level-sets method for semi-automatic brain tumor segmentation involves operator-selected tumor regions as initialization points, followed by iterative parameter adjustments and segmentation refinement through visual evaluation [18]. A neural network-based deformable model approach has been developed for enhanced segmentation performance [19]. It's important to note that the system is not a true 3D method, as the algorithm processes each slice separately [20]. Recent work has developed semi-automatic systems for brain tumor analysis, combining interactive extraction with classification capabilities while utilizing training and generalization processes for segmentation [21]. It's noteworthy that the inclusion of spatial features enhances the accuracy of classifiers such as KNN, SVM, or random forests [22]. A semi-automatic segmentation and classification approach has been developed using post-contrast T1-weighted MRI data [23]. Therefore, to facilitate the multiclass cancer tumors classification. The designed system comprises four main modules. For more detailed information, a comprehensive survey of various classification process employed in MRI images is elaborated [24].

While semi-automatic segmentation of brain tumors has proven to be less time-consuming compared to manual methods and can yield efficient results, it still remains susceptible to inter-and intra-rater or user variability [25]. Thus, recent investigations in brain tumor segmentation are predominantly focused on developing fully automatic methods [17]. In entirely automatic segmentation methods for brain tumors, there is no need for expert involvement. Typically, artificial intelligence (AI) and prior knowledge are amalgamated to address the segmentation challenge [17]. An automated brain tumor segmentation method incorporating Enhanced Darwinian Particle Swarm Optimization (EDPSO) has been developed to address limitations in conventional PSO approaches [26]. This novel method comprises three steps. The first step involves the removal of film artifacts and unwanted portions of MRI images utilizing a tracking procedure, along with the elimination of noise and highfrequency components through a Gaussian filter. In the second step, segmentation is performed using the Darwinian PSO method. The final step involves classification that is achieved through the Adaptive Neuro Fuzzy Inference System. Sehgal et al. [27] have proposed a fully automatic scheme for brain tumor segmentation, demonstrating high accuracy in tumor identification. The method employs the Fuzzy C-Means clustering algorithm for segmentation. This approach involves a preprocessing step, and area features along with circularity are utilized for the extraction of tumors from the segmented images.

Tejashwini et al. [28] propose SLCA-UNet, a modified UNet architecture for automated brain tumor segmentation in MRI images. The model integrates residual dense blocks, layered and channel attention, and stacked convolution to enhance feature extraction and reduce complexity. The model is tested on the BraTS 2020 dataset, it achieved good results in terms of sensitivity and specificity.

A hybrid algorithm combining SVM and FCM with contrast-enhanced preprocessing has been developed for brain tumor prediction [29]. Skull stripping is performed through both thresholding and morphological actions. The image segmentation step utilizes the FCM clustering algorithm. For feature extraction, the Grey Level Run Length Matrix (GLRLM) is employed. The classification of brain MRI images is then carried out using the Linear Quadratic with Polynomial SVM technique.

An effective segmentation method (AMSOMFKM) has been developed to address the challenges of tumor detection and extraction across diverse MR brain image datasets [30]. When it came to solving the tumor area segmentation problem, the proposed solution outperformed the AMSOM and FKM algorithms. By combining features taken from brain magnetic resonance imaging with previously acquired data. A brief overview of some existing methods for brain tumor recognition and segmentation is presented in Table 1.

Table 1. Representative existing studies on automated segmentation in brain tumor identification

Reference	Methods	Performance	
Lefohn et al. [18]	level-sets+Graphics Processing Units	Pre=94.04%	
Khan et al. [22]	marker-based watershed algorithm+SVM	Acc=92.26% Sen=91.01%	
Sachdeva et al. [23]	SROI+PCA	Over=95.85%	
Vijay et al. [26]	EDPSO+ANFIS	Pre=Acc=95%	
Sehgal et al. [27]	Fuzzy C- Means+Labeling of segmented Images	Dice=72.9 %	
Tejashwini et al. [28]	SLCA+UNet	Acc=98.95	
Parveen and Singh [29]	FCM+GLRLM+SVM	Spe=100% Sen=83.33%	

3. PROPOSED BRAIN TUMOR DETECTION FRAMEWORK

The proposed framework consists of three principal steps: segmentation, detection, and decision-making. Segmentation is performed using the FPSO algorithm, while detection is performed employing FCM. Decision-making is performed using a Mamdani-based fuzzy inference model. Figure 1 shows the phases of the proposed brain tumor segmentation technique using MRI images.

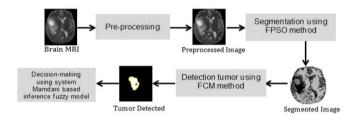


Figure 1. Proposed method diagram for brain tumor detection

3.1 Dataset

In this work, the objective is to generate a segmentation of the heterogeneous tumor region. To achieve this, two datasets were utilized, including the publicly available BRATS 2015 [31]. Furthermore, a private dataset was collected from the Civil Hospital of Setif, comprising 18 healthy and 18 unhealthy subjects. In the BRATS 2015 dataset, we specifically chose malignant tumors for segmentation and classification. A sample of the selected datasets is illustrated in Figure 2.

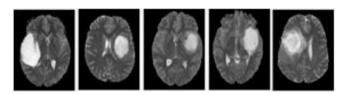
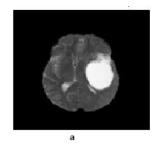


Figure 2. Brain tumor samples from the image dataset used in this study

3.2 Preprocessing

The preprocessing stage plays a significant role in

enhancing the quality of the image that leads to attaining good effects in segmentation processes.



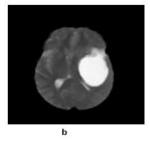


Figure 3. Preprocessing step: (a) Original MRI image and (b) Enhanced image after preprocessing

It consists of basic pre-processing techniques including adjusting image size, image normalization [32], image enhancement [31], image binarization and more [33]. Figure 3 shows the enhanced image after preprocessing

3.3 Fuzzy particle swarm optimization for segmentation

The segmentation process involves the method of partitioning an image into various homogeneous parts. Over the years, remarkable research progress in the field of brain tumor segmentation has been made. In this study, the FPSO is employed to segment the tumor zone from MRI brain. The selection of the FPSO is based on its simplicity, efficiency in segmentation applications, and its capability to handle information characterized by high-dimensional data [34].

The Particle Swarm Optimization (PSO) algorithm, developed in 1995, is an evolutionary computation technique inspired by natural swarm behavior that operates through iterative refinement [35]. In the PSO framework, a swarm consists of a set number of particles. In each iteration, these particles explore the N-dimensional problem space to evaluate and identify the global optimum. The velocity and position of each particle are updated according to the following equations:

$$V(t+1) = w.V(t) + c_1.rand_1.(Pbest(t) - X(t)) + c_2.rand_2.(Gbest(t) - X(t))$$
(1)

$$X(t+1) = X(t) + V(t+1)$$
 (2)

where,

- X denotes the position of the particle,
- V represents the particle's velocity,
- w is the inertia weight,
- The constants c_1 and c_2 are acceleration coefficients that regulate the influence of the particle's personal best (Pbest) and global best (Gbest) on the search process,
- r_1 and r_2 are random values between 0 and 1 [36].

The PSO algorithm faces a common challenge where particles can be trapped in local minima during convergence, leading to suboptimal solutions. This issue affects its ability to find the global minimum [37].

An enhanced fuzzy particle swarm optimization (FPSO) method has been developed to effectively solve the Traveling Salesman Problem [30]. This FPSO approach has since been applied to tackle fuzzy clustering challenges in image analysis [36, 38]. In this framework, the position of each particle (denoted by X) corresponds to the fuzzy membership values $\{p_1, p_2, ..., p_N\}$ of pixels to a set of cluster centers $\{C_1, C_2, ..., C_n\}$

 C_c }. The representation of X is as follows:

$$X = \begin{bmatrix} \mu_{11} & \cdots & \mu_{1c} \\ \vdots & \ddots & \vdots \\ \mu_{n1} & \cdots & \mu_{nc} \end{bmatrix}$$
 (3)

 u_{ij} indicates the degree of membership of the i-th pixel to the j-th cluster, based on certain constraints. The particle position matrix is structured similarly to the fuzzy matrix in the FCM. The particles' velocities are represented by a matrix V with dimensions (N, c), where N and c correspond to the number of rows and columns, respectively. The position and velocity updates in this process are determined by Eqs. (4) and (5) [39].

$$V(t+1) = w \otimes V(t) \oplus (c1r1) \otimes pbest(t) \ominus X(t)) \oplus (c2r2) \otimes (gbest(t) \ominus X(t))$$

$$(4)$$

$$X(t+1) = X(t) \oplus X(t+1) \tag{5}$$

The novel matrix by normalized values is supposed as follows [40]:

$$X_{normal} = \begin{bmatrix} \frac{\mu_{11}}{\sum_{j=1}^{c} \mu_{1j}} & \cdots & \frac{\mu_{1c}}{\sum_{j=1}^{c} \mu_{1j}} \\ \vdots & \ddots & \vdots \\ \frac{\mu_{n1}}{\sum_{j=1}^{c} \mu_{nj}} & \cdots & \frac{\mu_{nc}}{\sum_{j=1}^{c} \mu_{nj}} \end{bmatrix}$$
(6)

The FPSO method's fitness function evaluates generalized solutions, as defined in Eq. (7).

$$f(X) = \frac{K}{J_m} \tag{7}$$

where, K is a constant, J_m is the objective function of FCM method. The pseudo algorithm FPSO for fuzzy clustering problem is concise by Algorithm 1.

Algorithm 1. FPSO

Input: MRI Image.

- 1) Set the values for *P*, *c1*, *c2*, *w*, and the maximum iteration limit (itermax).
- 2) Create a swarm with P particles, where the matrices X, Pbest, Gbest, and V each have dimensions of n*c.
- 3) Initialize *X*, *V*, and *Pbest* for each particle, and set the global best *Gbest* for the swarm.
- 4) For t=1 to *itermax* do the following:
- 4.1 Determine the cluster centers for each particle based on Eq. (11).
- 4.2 Evaluate the fitness function for each particle based on Eq. (7).
 - 4.3 Update *Pbest* for each particle.
 - 4.4 Update *Gbest* for the swarm.
 - 4.5 Update V for each particle based on Eq. (4).
 - 4.6 Update X for each particle based on Eq. (5).
- 4.7 If the stopping condition has not been met, repeat from step 4.1.
- 5) End the iterations.

Output: Segmented image.

3.4 Tumor detection using Fuzzy C-Means

The subsequent steps involve the separation of outlier data, as previously mentioned, with the segmented image aiming to highlight the tumor. A non-supervised Fuzzy C-Means

algorithm approach is employed. This choice is because of its success in different domains, such as image analysis and medical diagnosis. Despite its low complexity and simple implementation, especially for large datasets [41], the FCM algorithm has proven to be fruitful for segmenting brain tumors. FCM is an unsupervised fuzzy clustering algorithm, classified as a constrained soft clustering algorithm. The approach is based on minimizing a quadratic criterion [40]. In the FCM algorithm, data point membership to clusters is based on their proximity to cluster centers, aiming to minimize an objective function related to the fuzzy membership set U and centroids V [41].

$$J = \sum_{i=1}^{C} \sum_{j=1}^{N} (u_{ij})^{m} d^{2}(x_{j}, c_{i})$$
 (8)

With the following constraint:

$$\forall j \in [1, N]: \sum_{i=1}^{C} u_{ij} = 1$$

$$\forall i \in [1, C], \forall j \in [1, N]: u_{ij} \in [0, 1]$$
(9)

In these equations, u_{ij} represents the membership of pixel x_j for the j-th cluster, where c_i is the center of the i-th cluster. Additionally, $d(x_j, c_i)^2$ is the Euclidean distance between x_j and c_i . The parameter m, which is greater than 1, directs the resulting partition' fuzziness. The cluster centers and membership functions are updated using Eq. (10) and Eq. (11), respectively.

$$u_{ij} = \left[\sum_{k=1}^{C} \left(\frac{d(x_j, b_i)}{d(x_j, b_k)} \right)^{\frac{2}{(m-1)}} \right]^{-1}$$
 (10)

$$b_{i} = \frac{\sum_{k=1}^{N} (u_{ik}^{m} + t_{ik}^{\lambda}) x_{k}}{\sum_{k=1}^{N} (u_{ik}^{m} + t_{ik}^{\lambda})}$$
(11)

The FCM algorithm iteratively repeats two basic conditions till a solution is obtained. The final phase of segmentation is achieved by allocating data points to the cluster with the most significant membership value [42]. The steps of this algorithm are considered as follows:

Algorithm 2. FCM

Input: A set of image segments segmented by FPSO.

- 1). Ensemble of values of the number of clusters c, the fuzziness degree m and the error *epsilon* (ε) .
 - 2). For i=1, 2, ..., c:

Compute the center of the fuzzy cluster c_i , using Eq. (11).

- 3). Update the fuzzy membership u_{ij} using Eq. (10).
- 4). If the value of J is smaller than the predefined threshold ε , stop; otherwise, return to step 2.

Output: Tumor detection.

3.5 Decision-making

At the final stage, the objective is to determine if a given pixel corresponds to a brain tumor or not. To accomplish this, a Mamdani model based fuzzy inference system has been implemented. The Mamdani Fuzzy Inference System offers a robust framework for integrating expert knowledge into the decision-making process. It is composed of rules structured as "IF... THEN..." statements, and the relationships between rules

are expressed using "AND" and "OR" connectors [43]. In the proposed algorithm, a fuzzy inference system of the Mamdani type is employed based on expert knowledge to generate a knowledge base. This imparts the system with the ability to make decisions using the rules created in the knowledge base for the system's output. Brain tumors typically appear either hypointense in the T1-w sequence or hyperintense in T2-w and PD-w sequences [44]. The proposed Mamdani fuzzy inference system for the evaluation of brain tumor risk comprises two inputs: the contrast of MR Image and the signal of tumor detection. The system has one output that indicates the risk of brain tumor (refer to Figure 4).

Depending on the characteristics of the input signal, two membership functions are defined: 'hyposignal' and 'hypersignal', as illustrated in Figure 5.

Based on the output for brain tumor classification, three Gaussian membership functions are utilized to represent the tumor states: high, normal, and low, as illustrated in Figure 6.

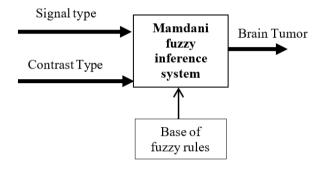


Figure 4. Diagram of the fuzzy inference system implemented in our approach

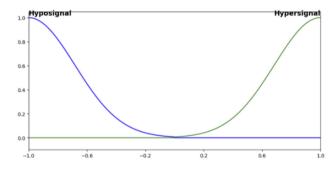


Figure 5. Membership functions for different signal types

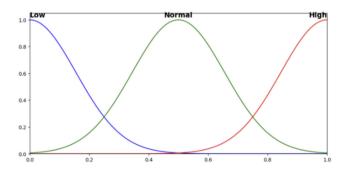


Figure 6. Gaussian membership functions for brain tumor classification

The fuzzy rules set for MIN-MAX Mamdani fuzzy inference system are defined as follows:

• If [(The contrast is T1-w) AND (The signal is hypersignal)], then (The tumor is low).

- If [(The contrast is T1-w) AND (The signal is hypersignal)], then (The tumor is middling).
- If [(The contrast is T2-w) AND (The signal is hypersignal)], then (The tumor is high).
- If [(The contrast is PD-w) AND (The signal is hypersignal)], then (The tumor is high).
- If [(The contrast is T1-w) AND (The signal is hyprosignal)], then (The tumor is low).
- If [(The contrast is T2-w) AND (The signal is hyporsignal)], then (The tumor is high).
- If [(The contrast is PD-w) AND (The signal is hyporsignal)], then (The tumor is high).

In this work, we opted for the MIN-MAX Mamdani inference system. This model employs the connective operators AND and OR to implement min and max, respectively. We used Tanaka's proposed Center of Gravity strategy as the defuzzification method [45] for our case studies, which turns the fuzzy set produced by inference into a numerical value by taking into account all possible outputs.

3.6 Evaluation metrics

To assess the capability of the proposed brain tumor segmentation, three metrics are computed: sensitivity, Jaccard index, Accuracy and specificity. These metrics are defined by the following equations [46]:

$$Jaccard = \frac{TP}{TP + FN + FP}$$
 (12)

Sensitivity =
$$\frac{TP}{TP + FN}$$
 (13)

Specificity =
$$\frac{TN}{TN + FP}$$
 (14)

$$Accuracy = \frac{TP + TN}{TP + TN + FN + FP}$$
 (15)

where,

- TP (True Positive) refers to the total number of pixels correctly segmented as tumor pixels,
- FP (False Positive) represents the total number of pixels incorrectly segmented as tumor pixels,
- FN (False Negative) is the number of pixels mistakenly classified as healthy,
- TN (True Negative) indicates the total number of pixels correctly identified as healthy pixels [3].

4. RESULTS AND DISCUSSION OF THE EXPERIMENTS

4.1 Brain tumor segmentation and detection using FPSO and FCM algorithms

To assess the performance of each employed segmentation algorithm (FPSO, FCM, and FPSOFCM), corresponding to specific stages in the proposed pipeline for brain tumor segmentation, axial slices of the original MRI images are presented in Figure 7. The rows in the figure depict: (a) Original MRI images before segmentation, (b) Segmented images using the FPSO algorithm showing different tissues, and (c) Tumor extraction using the FCM algorithm in the final

stage, where the number of clusters (c) was set to 2 and the fuzziness parameter (m) was set to 2.0 to ensure reproducibility.

The impact of each result on the proposed approach is assessed by analyzing the improvements in sensitivity, specificity, and Jaccard index performance metrics. Table 2 presents the quantitative results of these evaluations.

Table 2 presents the performance evaluation measures, including the Jaccard index, sensitivity, and specificity, for MRI brain tumor images using the proposed segmentation technique for brain tumor diagnosis. The results indicate that the proposed approach (FPSOFCM) is both effective and clinically acceptable. Specifically, the Jaccard index shows promising results, with an average of 0.85 across the datasets. The sensitivity values have an average of 0.92, while the specificity values show an average of 0.97.

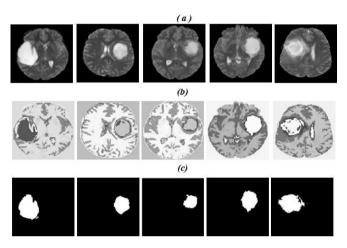


Figure 7. Scheme of the complete brain tumor segmentation process: (a) Original MR images, (b) Segmented images using FPSO, and (c) Brain tumor detection using FCM

Table 2. Value of Jaccard, sensitivity and specificity for brain tumor segmentation

Performances (Tumors Detected)	Jaccard	Sensitivity	Specificity
Brain tumors	0.85	0.92	0.97

4.2 Decision-making process

In this step, the output result aids in making decisions for brain tumor detection. The fuzzy inference system requires concepts characterized in membership functions, logical operations, and rule-based structures. The fuzzy inference process starts with fuzzification and ends with defuzzification. In our proposed Mamdani model based fuzzy inference, MIN and MAX operators are implemented. The potential brain tumors detected are progressed via this inference system that acts as an expert in determining whether a pixel belongs to the brain tumor cluster or not. Table 3 reports the achieved results considering the three MRI sequences.

Table 3. Defuzzification results on different MRI sequences.

MRI Sequences/ Tumors Detected	T1-w (%)	T2-w (%)	PD-w (%)
Brain Tumor	53.53	88.17	77.04

Proactive identification and treatment of brain tumors are

vital for successful management. Decision-making in clinical applications heavily relies on expertise. From Table 3, it is evident that the patient has a brain tumor. The tumors are identified in all sequences of MRI images with a high level of description.

4.3 Comparative study

Here, we illustrate comparative study of the offered algorithm with the FPSO and FCM algorithms by employing an ensemble of MRI brain images for brain tumor detection. The segmentation results of a sample of selected datasets are illustrated in Figure 8.

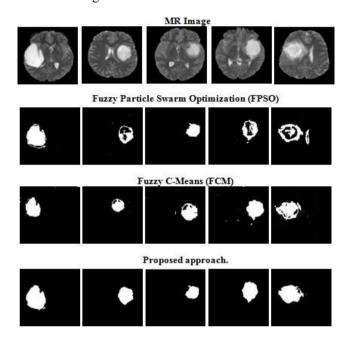


Figure 8. Segmentation results obtained using various methods

In this proposed technique we got 99.71% accuracy that is good than the state of the art results obtained by the studies [22, 28, 25, 30] as shown in the Table 4.

Table 4. Comparison of segmentation performance

References	Techniques	Accuracy %
[30]	AMSOM+FKM	99.8
	MARKER-BASED	
[22]	WATERSHED ALGORITHM +	93.29
	SVM	
[28]	SLCA+UNet	98.95
[25]	SVM+CNN	99.74
Proposed approach	FPSO+FCM	99.71

5. CONCLUSIONS

Detecting and identifying tumors from MRI images quickly, accurately, and reproducibly remains a challenging problem. Brain tumor segmentation has shown immense potential in identifying and examining tumors in medical imaging, and this trend is expected to persist in the future. Therefore, this paper presents a fully automated method for brain tumor detection. The combination of FCM algorithms and FPSO was utilized for brain tumor segmentation. Experimental results

demonstrated that the segments extracted by the FPSOFCM algorithm from MRI images outperformed those obtained by classical methods (FPSO and FCM). Furthermore, in a comparative study with previous existing works, all three presented approaches achieved higher performances. In conclusion, the high accuracy of the proposed FPSOFCM method makes it a promising system for brain tumor diagnosis in a clinical setting based on MRI images. In future work, we plan to extend this system by incorporating other hybrid techniques, including combining FPSO/FCM with deep learning models such as Convolutional Neural Networks (CNNs) or Transformer-based architectures, to further enhance brain tumor detection performance. Additionally, the proposed method will be further analyzed for its applicability to other areas of biomedical image processing.

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